

Higher-Order Wavefront Aberrations for Populations of Young Emmetropes and Myopes

Jinhua Bao¹, Rongrong Le¹, Jiangxiu Wu¹, Yeyu Shen¹, Fan Lu¹ and Ji C. He^{1,2}

ABSTRACT

PURPOSE: To test the hypothesis that human eyes have a central tendency to be free of higher-order aberrations by analyzing wavefront aberrations for two young populations of respectively emmetropic and myopic subjects.

METHODS: Both right and left eyes of 75 emmetropes and 196 myopes were measured for corneal wavefront aberration using a Humphrey corneal topographer and for the whole eye wavefront aberration using a WASCA wavefront sensor without pupil dilation. 35 Zernike aberration coefficients over a 6.0 mm pupil diameter were derived, and statistics of the higher-order terms (3rd to 5th orders) were tested.

RESULTS: When signed Zernike aberrations of the right and left eyes were averaged together for the emmetropes, three higher-order modes ($j=6, 12$ and 13) were significantly different from zero in both the cornea and the whole eye ($P<0.0005$), and three additional terms ($j=14, 15$ and 17) were statistically non-zero for the whole eye. As the signs of y -axis asymmetrical terms in the left eye were flipped, three more terms in either the cornea ($j=8, 18$ and 19) or the whole eye ($j=8, 10$ and 20) became statistically non-zero. For the myopes, 8 corneal terms and 5 whole-eye terms were statistically non-zero when the two eyes were averaged together. As the signs flipped, the majority of the Zernike aberration terms were statistically different from zero.

CONCLUSIONS: Human eyes have systematical higher order aberrations in population, and factors that cause bilateral symmetry of wavefront aberrations between the right and left eyes made important contribution to the systematical aberrations.

(J Optom 2009;2:51-58 ©2009 Spanish Council of Optometry)

KEY WORDS: higher order aberration; Zernike aberration; emmetropia; myopia; bilateral symmetry.

RESUMEN

OBJETIVO: Poner a prueba la hipótesis de que el ojo humano, en promedio, tiende a estar libre de aberraciones de alto orden. Para ello se analizó la aberración de onda en dos poblaciones distintas: una compuesta por jóvenes emétopes, la otra por jóvenes miopes.

MÉTODOS: Se estudiaron los ojos izquierdo y derecho de 75 emétopes y de 196 miopes. En cada ojo, sin dilatar la pupila, se midieron las aberraciones corneales utilizando un topógrafo corneal Humphrey y también se obtuvo la aberración de onda de toda la óptica ocular por medio de un sensor de frente de onda WASCA. A partir de estos datos se calcularon los 35 coeficientes de aberración de Zernike que caracterizan cada patrón de aberración para un diámetro de pupila

de 6,00 mm, realizándose a continuación un análisis estadístico de los términos de alto orden (del 3^o al 5^o orden).

RESULTADOS: Cuando para los emétopes se promedian los coeficientes de aberración de Zernike para los ojos izquierdo y derecho, manteniendo su signo, hay tres modos de alto orden ($j=6, 12$ y 13) que resultan ser significativamente distintos de cero, tanto para la córnea como para todo el ojo. Además, otros tres términos ($j=14, 15$ y 17) resultaron ser también estadísticamente distintos de cero cuando se analiza todo el ojo en su conjunto. Cuando se cambia para el ojo izquierdo el signo de los coeficientes correspondientes a los términos de aberración que son asimétricos respecto al eje y , hay tres términos más (en la córnea: $j=8, 18$ y 19 , y para todo el ojo: $j=8, 10$ y 20) que pasan a ser estadísticamente distintos de cero. En lo que respecta a los miopes, hay 8 términos para la córnea y 5 términos para todo el ojo que resultan ser estadísticamente distintos de cero cuando se promedian los dos ojos de todos los integrantes del grupo. Cuando se cambian los signos, de forma análoga al grupo anterior, la mayoría de los coeficientes de aberración de Zernike resultan ser estadísticamente distintos de cero.

CONCLUSIONES: El ojo humano presenta de forma sistemática aberraciones de alto orden. Los factores que provocan la simetría bilateral de la aberración de onda entre el ojo izquierdo y derecho de cada individuo contribuyen de manera importante a la presencia de dichas aberraciones sistemáticas.

(J Optom 2009;2:51-58 ©2009 Consejo General de Colegios de Ópticos-Optometristas de España)

PALABRAS CLAVE: aberraciones de alto orden; aberraciones de Zernike; emetropía; miopía; simetría bilateral.

INTRODUCTION

Recent improvements in aberrometry have made a fast and precise measurement of wavefront aberrations in the human eye possible not only in the laboratory for eye research but also in the offices of optometry and ophthalmology for clinical diagnosis. Consequently, a number of studies have been conducted to investigate the nature of wavefront aberrations in the human eye (e.g. see reviews by Applegate,¹ Thibos,² and Charman³). For the normal population, the human eye has been believed to have a central tendency to be free of higher-order aberrations, because the mean of the higher-order Zernike modes, excluding the spherical aberration,^{3,4} for each individual Zernike term, were not significantly different from zero, even though none of the higher-order aberrations for a single eye was by any means equal to zero. Results supporting the hypothesis of the population being free of higher-order aberrations arose mainly from three population studies that used experimental systems constructed in the laboratory.⁴⁻⁶ If the hypothesis was true, it could imply, from the viewpoint of eye research, that the eye is very well corrected of its higher-order aberrations under the pressure of nature selection, despite the existence of subs-

From the ¹Wenzhou Medical College, 82 Xueyuan Road, Wenzhou, Zhejiang 325027, China, ²New England College of Optometry, 424 Beacon Street, Boston, MA 02115, USA

Acknowledgment: This study was supported by Chinese National Key Technologies R&D Program Grant (2004BA720A16) and Zhejiang Province Key R&D Program Grant (2005C14001).

Received: 21 October 2008

Revised: 9 January 2009

Accepted: 11 January 2009

Corresponding author: J.H. Wenzhou Medical College, 82 Xueyuan Road, Wenzhou, Zhejiang 325027, China. e-mail: hej@neco.edu.

TABLE 1

Information regarding number of subjects N, mean \pm SD of age (year), mean \pm SD of refractive error (D) and aberrometers used in previous population studies. "Setup" under "aberrrometer" means experimental setup

	N (Eye)	Age (Range)	Refraction (Range)	Aberrometer
Thibos et al. ⁴	100(200)	26.1 \pm 5.6 (22-35)	-3.1 \pm 3.0 (-12.0 to 6.00)	Setup
Porter et al. ⁵	109(218)	41 (21-65)	(-12.0 to 6.00)	Setup
Castejon-Mochon et al. ⁶	59(108)	24 \pm 3 (20-30)		Setup
He et al. ⁷	316(632)	17.8 (10-29)	-1.49 (-9.0 to 0.75)	Setup
Carkeet et al. ⁸	273(273)	9.0 \pm 0.84 (7.9-10.7)	-1.00 \pm 1.92	Zywave
Wang & Koch ⁹	306(532)	41 \pm 10 (20-71)	-3.39 \pm 2.84 (-11.56 to 7.60)	WaveScan
Brunette et al. ¹⁰	114(114)	43.2 \pm 24.5 (5.7-82.3)	-0.03 \pm 1.58 (-3.50 to 3.50)	Setup
Amano et al. ¹¹	75(75)	43.5 \pm 11.7 (18-69)	-1.77 \pm 3.26 (-10.00 to 3.50)	KR-9000PW
Cheng et al. ¹²	76(76)	24.8 \pm 4.0 (21-40)	-2.50 \pm 2.25 (-8.25 to 1.25)	Setup
Netto et al. ¹³	226(418)	42.8 \pm 10.5 (20-67)	-3.40 \pm 3.10 (-10.70 to 5.4)	WaveScan
Zadok et al. ¹⁴	36 (61)	22 (18-43)	-2.50 \pm 2.36 (-10.25 to -0.25)	WaveScan
Wei et al. ¹⁵	166(166)	32.1 \pm 6.2 (21.5-52.8)	-5.23 \pm 1.79 (-9.75 to -0.75)	Zywave
Plainis et al. ¹⁶	218(393)	33 \pm 4.8 (21-43)	-0.25 \pm 0.47 (-1.25 to 1.13)	Wavelight

tantial individual variation. Meanwhile, from the viewpoint of clinical practice, the optimal goal for eye treatment is to correct the higher-order aberrations completely.

However, besides the three aforementioned laboratory studies,^{4,6} several other wavefront measurements with a large sample size have also been recently documented in the literature.⁷⁻¹⁶ Table 1 summarizes the basic information on sample size, age, refraction and techniques used in each of the studies. In those later studies, five of them^{7-9,15-16} reported mean Zernike coefficients, and four experiments were conducted using commercial aberrometers. Carkeet and colleagues⁸ statistically tested the mean of the higher-order Zernike aberrations (3rd to 5th order), and found 10 out of 15 Zernike terms to be significantly different from zero. Taking the mean Zernike coefficients and standard deviations reported by Wang and Koch⁹ and by Wei et al.¹⁵ as starting point, we have made a statistical test using their data with multi-comparison correction and found that about 2/3 of the Zernike terms were significantly different from zero. Plainis and Pallikaris¹⁶ only reported mean higher-order Zernike aberrations taking the right and left eyes separately. A reanalysis of their data with multi-comparison correction revealed that three higher-order Zernike terms, including spherical aberration, were significantly different from zero when both eyes were averaged together. Obviously, the hypothesis stating that human eyes show a central tendency to be free of higher-order aberrations was not supported in the four later population studies.^{8-9,15-16}

Yet, there were differences between these four later studies^{8-9,15-16} and the three early laboratory studies,^{4,6} such as the systems used to measure aberrations, subject age and refraction, and even the usage of cycloplegia. While the experimental systems for the three early studies were constructed in the laboratory, the aberrometers used in the four later studies were commercial models. It is quite possible that different systems might have different accuracy and precision, thus resulting in different data.

In order to test the hypothesis of a population having eyes free of higher-order aberrations, we have measured the wavefront aberrations for a group of young adults using a commercial aberrometer (WASCA Wave-front Analyzer), which has been experimentally tested for its accuracy and precision in a previous study.¹⁷ For a better understanding of the nature of higher-order aberrations in a normal population, this study was focused on emmetropes, because it is more reasonable to test the hypothesis in normal emmetropic eyes rather than in eyes with refractive errors. The subjects in the study of Plainis & Pallikaris¹⁶ were emmetropes also, but only three higher-order Zernike aberrations were found to be statistically different from zero. In addition, we have also tested a group of young myopes for comparison. Moreover, wavefront aberrations in the anterior corneal surface were examined using a precisely calibrated corneal topography system,^{18,19} because the anterior cornea plays an important role in determining wavefront aberrations in the whole eye.^{18,20-23}

METHOD

Subjects

Emmetropic subjects were recruited among students of the Wenzhou Medical College (WMC) and among students from the Wenzhou police school. Myopic subjects were recruited from the WMC and the candidates for refractive surgery in the Refractive Surgery Center of Eye hospital, WMC. Best corrected visual acuity (BCVA) for all subjects was 20/25 or better. Subjects with any ocular pathology or having astigmatism greater than 2.5D were excluded. The final subject number in this study was 75 in the emmetropic group and 196 in the myopic group.

Refraction was measured with the use of cycloplegia. The emmetropes were aged 18 to 33 yrs (mean = 21.7 \pm 3.4 yrs) and had spherical errors ranging from -0.50 to +1.25 D (mean = 0.13 \pm 0.37D), including the subjects with -0.5D in only one eye, and cylinder from -2.00 to 0.00D (mean

= -0.36 ± 0.29 D). Only one subject had spherical error equal to 1.25D, and the rest had values equal or less than 0.75D. The myopes were aged 18 to 38 yrs (mean = 25.2 ± 5.0 yrs), and had spherical errors ranging from -10.0 to -0.5D (mean = -4.70 ± 2.14 D), including the subjects that had -0.5D in both eyes, and a cylinder from -2.50 to 0.00D (mean = -0.64 ± 0.56 D). The research followed the tenets of the Declaration of Helsinki, and was approved by the Committee of Ethics of Wenzhou Medical College.

Instruments

A Humphrey ATLAS Corneal Topography System (Carl Zeiss Meditec, Germany) was used to measure corneal aberrations. The system directly provided estimates of the pupil margin, pupil center location, vertex location, curvatures of the anterior corneal surface, and keratometric measurements. We have used the corneal curvatures and corneal heights, exported from the ATLAS system, to calculate corneal aberrations. Wavefront aberrations in the whole eye were measured using a WASCA Wavefront Analyzer (Carl Zeiss Meditec, Germany), from which refractive error and a series of Zernike aberration terms, up to 7th order, were directly obtained. According to Salmon et al.'s study,¹⁷ the repeatability of the WASCA system for 3rd, 4th, 5th, 6th and 7th order aberrations were 0.035, 0.025, 0.020, 0.015 and 0.010 μ m respectively.

Experimental Procedure

The experiment was performed with room lights off. No mydriatics were used. For each subject, four corneal topographies over a 10.0 mm zone were taken first, followed by three measurements of the wavefront aberrations of the whole eye. Most subjects had a pupil size greater than 6.0 mm during the measurements of whole-eye aberrations. For those subjects whose pupil size was less than 6.0 mm, the data was excluded from further analysis. The right and left eyes were tested in random order, and for each subject it took about 10 minutes to complete the experiments.

Data Analysis

From the corneal heights, exported from the ATLAS system, wavefront aberrations for the anterior cornea were calculated using a customized MatLab ray-tracing program¹⁸⁻¹⁹ to derive Zernike aberration terms up to the 7th order (35 terms). The corneal height data were originally referenced to corneal vertex in the ATLAS system. In order to describe the corneal aberrations with respect to the line of sight of the eye, as it is done for the whole-eye aberrations, a transformation of the coordinate center from the corneal vertex to the pupil center was performed with the customized program, using the pupil center measurements provided by the ATLAS system. After the transformation, corneal height data over a 6.0 mm diameter area, relative to the pupil center, were used to calculate corneal Zernike aberrations with ray-tracing and Gram-Schmidt orthogonalization procedures.¹⁸ For each eye, the mean of three measurements of either the anterior cornea or the whole eye over a 6.0 mm pupil area was calculated and taken as the

final estimate of the aberrations. The single-index conversion was used to name the Zernike aberrations.²⁴ Statistical analyses were performed using SPSS 13.0.

RESULTS

Mean Higher-Order Zernike Aberrations for Emmetropes

When both the right and the left eyes were accounted together, the resulting mean signed Zernike aberrations in the anterior cornea and the whole eye for 75 emmetropic subjects are as listed in *table 2*, where only 3rd to 5th orders were included. All other higher order aberrations (6th to 7th) were not given in *table 2* because the mean absolute values or magnitudes were very small ($< 0.01 \mu$ m). The results of the t-test at a 95% confidence interval and *P*-value (uncorrected for multi-comparison) for the mean values being different from zero are also listed in *table 2*. Significance corrected for multi-comparison was indicated with asterisks for the corresponding levels. As depicted in *table 2*, three Zernike terms ($j = 6, 12$ and 13) were significantly different from zero in both the anterior cornea and the whole eye simultaneously. Three additional modes ($j = 14, 15$ and 17) were different from zero only in the whole eye. While the spherical aberration ($j = 12$) both in the anterior cornea and in the whole eye was positive, the aberration coefficients corresponding to $j=6$ and 13 were always negative. The absolute values in the anterior cornea were always greater than those in the whole eye for these three Zernike aberrations ($j = 6, 12$ and 13). For the three non-zero Zernike aberrations in the whole eye only, the mean amplitude of the 4th order aberration ($j = 14$) was relatively large ($>0.04 \mu$ m) while the levels of the other two 5th order terms ($j = 15$ and 17) were around or less than 0.01μ m.

Bilateral symmetry of wavefront aberrations between the right and left eyes both in the anterior cornea and in the whole eye has been well documented in literature.^{5-6,9,13,23,25-30} With bilateral symmetrical structure, the sign of Zernike coefficients in the right eye is opposite to that in the left eye for those Zernike terms that are asymmetrical with respect to the *y*-axis, those corresponding to $j=8, 9, 10, 11, 18, 19$ and 20 . To account for the effect of bilateral symmetry on statistical analysis, the sign in the left eye is usually flipped before an average of the two eyes was made. *Table 3* shows the mean Zernike aberrations for the emmetropes with the signs in the left eye flipped. Because the sign flipping was restricted to the seven *y*-axis asymmetrical terms, the results in *table 3* therefore differ from those in *table 2* only in these seven terms. As shown in *table 3*, three more terms in either the cornea ($j=8, 18$ and 19) or the whole eye ($j=8, 10$ and 20) become significantly different from zero.

Root-mean-square (RMS) of the higher-order aberrations (3rd to 5th orders) for both the right and the left eyes were calculated for the 75 emmetropes, and the mean RMS for all 150 eyes was equal to 0.411μ m in the anterior cornea and to 0.336μ m in the whole eye. When spherical aberration was excluded from the RMS calculation, the mean RMS values decreased to 0.337μ m and 0.284μ m respectively. The RMS of mean higher order aberrations was also calculated according to the mean Zernike values in *table 2* and *3*. Without flipping

TABLE 2

Mean higher-order Zernike aberrations of the anterior cornea and of the whole eye over a 6.0 mm pupil area for 76 young emmetropes, with signed coefficients from both right and left eyes averaged together

	Anterior Cornea			Whole Eye		
	Mean \pm SD (μm)	95% CI (μm)	<i>P</i>	Mean \pm SD (μm)	95% CI (μm)	<i>P</i>
j=6 (Z_3^{-3})	-0.069 \pm 0.149	(-0.093, -0.046)	<0.0001***	-0.048 \pm 0.155	(-0.073, -0.024)	0.0001**
j=7 (Z_3^{-1})	-0.007 \pm 0.191	(-0.037, 0.024)	0.656	0.009 \pm 0.177	(-0.019, 0.037)	0.544
j=8 (Z_3^1)	0.009 \pm 0.167	(-0.018, 0.035)	0.522	0.008 \pm 0.092	(-0.007, 0.023)	0.287
j=9 (Z_3^3)	-0.006 \pm 0.118	(-0.025, 0.013)	0.513	-0.004 \pm 0.100	(-0.019, 0.012)	0.661
j=10 (Z_4^{-4})	-0.004 \pm 0.063	(-0.014, 0.006)	0.465	0.004 \pm 0.039	(-0.002, 0.010)	0.226
j=11 (Z_4^{-2})	0.001 \pm 0.041	(-0.006, 0.007)	0.853	-0.005 \pm 0.036	(-0.011, 0.001)	0.097
j=12 (Z_4^0)	0.218 \pm 0.073	(0.206, 0.229)	<0.0001***	0.137 \pm 0.122	(0.118, 0.156)	<0.0001***
j=13 (Z_4^2)	-0.037 \pm 0.081	(-0.050, -0.024)	<0.0001***	-0.017 \pm 0.058	(-0.026, -0.008)	0.0004**
j=14 (Z_4^4)	-0.007 \pm 0.065	(-0.017, 0.003)	0.189	0.041 \pm 0.052	(0.032, 0.049)	<0.0001***
j=15 (Z_5^{-5})	-0.013 \pm 0.069	(-0.024, -0.002)	0.020	-0.010 \pm 0.030	(-0.015, -0.005)	<0.0001***
j=16 (Z_5^{-3})	-0.000 \pm 0.045	(-0.008, 0.006)	0.867	0.002 \pm 0.030	(-0.003, 0.006)	0.478
j=17 (Z_5^{-1})	0.000 \pm 0.095	(-0.015, 0.015)	0.968	0.009 \pm 0.036	(0.003, 0.015)	0.003*
j=18 (Z_5^1)	-0.004 \pm 0.034	(-0.009, 0.002)	0.165	-0.002 \pm 0.021	(-0.005, 0.001)	0.229
j=19 (Z_5^3)	0.000 \pm 0.035	(-0.006, 0.006)	0.972	0.001 \pm 0.018	(-0.002, 0.004)	0.398
j=20 (Z_5^5)	-0.002 \pm 0.048	(-0.010, 0.005)	0.555	0.001 \pm 0.029	(-0.004, 0.005)	0.960

Significance was corrected for multi-comparison with * standing for $P < 0.05$ (0.0033), ** for $P < 0.01$ (0.00067), and *** for $P < 0.001$ (0.000067) level respectively.

TABLE 3

Mean-higher order Zernike aberrations of the anterior cornea and of the whole eye over a 6.0 mm pupil area for 76 young emmetropes, with signed coefficients averaged for both right and left eyes but the signs flipped for the y-axis asymmetrical Zernike coefficients in the left eye

	Anterior Cornea			Whole Eye		
	Mean \pm SD (μm)	95% CI (μm)	<i>P</i>	Mean \pm SD (μm)	95% CI (μm)	<i>P</i>
j=6 (Z_3^{-3})	-0.069 \pm 0.149	(-0.093, -0.046)	<0.0001***	-0.048 \pm 0.155	(-0.073, -0.024)	0.0001**
j=7 (Z_3^{-1})	-0.007 \pm 0.191	(-0.037, 0.024)	0.656	0.009 \pm 0.177	(-0.019, 0.037)	0.544
j=8 (Z_3^1)	-0.124 \pm 0.110	(-0.141, -0.106)	<0.0001***	-0.031 \pm 0.088	(-0.045, -0.017)	<0.0001***
j=9 (Z_3^3)	-0.013 \pm 0.109	(-0.030, 0.005)	0.150	0.015 \pm 0.100	(-0.001, 0.031)	0.060
j=10 (Z_4^{-4})	-0.004 \pm 0.053	(-0.012, 0.005)	0.364	0.013 \pm 0.036	(0.008, 0.019)	<0.0001***
j=11 (Z_4^{-2})	-0.006 \pm 0.035	(-0.011, 0.000)	0.042	-0.008 \pm 0.035	(-0.013, -0.002)	0.007
j=12 (Z_4^0)	0.218 \pm 0.073	(0.206, 0.229)	<0.0001***	0.137 \pm 0.122	(0.118, 0.156)	<0.0001***
j=13 (Z_4^2)	-0.037 \pm 0.081	(-0.050, -0.024)	<0.0001***	-0.017 \pm 0.058	(-0.026, -0.008)	0.0004**
j=14 (Z_4^4)	-0.007 \pm 0.065	(-0.017, 0.003)	0.189	0.041 \pm 0.052	(0.032, 0.049)	<0.0001***
j=15 (Z_5^{-5})	-0.013 \pm 0.069	(-0.024, -0.002)	0.020	-0.010 \pm 0.030	(-0.015, -0.005)	<0.0001***
j=16 (Z_5^{-3})	-0.000 \pm 0.045	(-0.008, 0.006)	0.867	0.002 \pm 0.030	(-0.003, 0.006)	0.478
j=17 (Z_5^{-1})	0.000 \pm 0.095	(-0.015, 0.015)	0.968	0.009 \pm 0.036	(0.003, 0.015)	0.003*
j=18 (Z_5^1)	-0.006 \pm 0.024	(-0.010, -0.002)	0.002*	-0.000 \pm 0.020	(-0.004, 0.003)	0.869
j=19 (Z_5^3)	-0.007 \pm 0.027	(-0.011, -0.003)	0.002*	-0.004 \pm 0.018	(-0.006, -0.001)	0.015
j=20 (Z_5^5)	0.005 \pm 0.039	(-0.001, 0.012)	0.083	0.012 \pm 0.026	(0.007, 0.016)	<0.0001***

Significance was corrected for multi-comparison with * standing for $P < 0.05$ (0.0033), ** for $P < 0.01$ (0.00067), and *** for $P < 0.001$ (0.000067) level respectively.

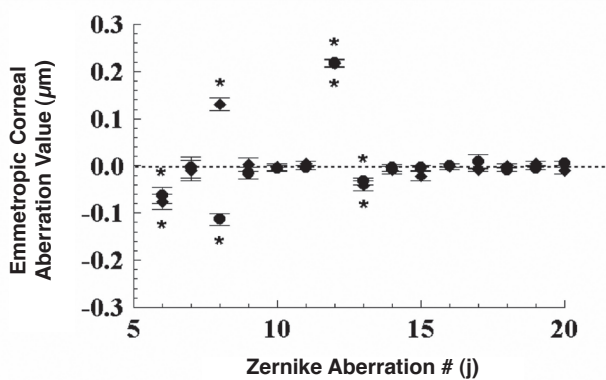


FIGURE 1
Mean higher-order Zernike aberrations of the anterior corneal surface over a 6.0 mm pupil area for the right (solid circles) and left eyes (solid diamonds) of 76 emmetropes.

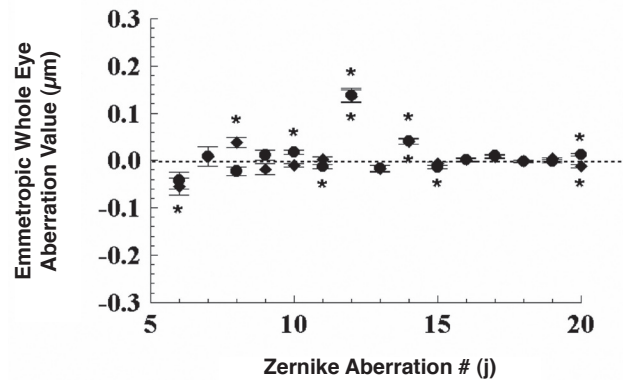


FIGURE 2
Mean higher-order Zernike aberrations of the whole eye for the right (solid circles) and left eyes (solid diamonds) of 76 emmetropes.

the signs (*Table 2*), the RMS of higher-order aberration terms was equal to 0.233 μm (in the cornea) and 0.155 μm (in the whole eye) when spherical aberration was included, and 0.079 μm (in the cornea) and 0.070 μm (in the whole eye) when spherical aberration was excluded. After the signs were flipped, the higher-order RMS values became 0.264 μm (in the cornea) and 0.159 μm (in the whole eye) with spherical aberration included, and 0.147 μm (in the cornea) and 0.080 μm (in the whole eye) when spherical aberration was excluded.

Figure 1 shows the mean corneal Zernike aberrations in the right (solid circles) and the left eye (solid diamond) for the 75 emmetropes, with the error bars standing for \pm one standard error of the mean, when the data from the two eyes was analyzed separately. There were 4 Zernike terms significantly different from zero: those corresponding to $j = 6$ ($t=3.56$, $P=0.0006$ for OD; $t=4.55$, $P=0.0002$ for OS), 8 ($t=9.03$, $P<0.0001$ for OD; $t=9.68$, $P<0.0001$ for OS), 12 ($t=27.46$, $P<0.0001$ for OD; $t=24.63$, $P<0.0001$ for OS) and 13 ($t=4.39$, $P<0.0001$ for OD; $t=3.86$, $P=0.0002$ for OS) both for the right and left eyes. The horizontal coma ($j = 8$) was significantly different between the right and left eyes also ($t=13.24$, $P<0.0001$). It can be seen in *figure 1* that the mean magnitude of the horizontal coma (-0.11 ± 0.11 μm for OD and 0.13 ± 0.12 μm for OS) is large compared to other higher-order aberrations, except of the spherical aberration (0.22 ± 0.07 μm for OD and 0.22 ± 0.08 μm for OS).

Figure 2 shows the mean higher-order Zernike aberrations in the whole eye for the 75 emmetropes with the two eyes analyzed separately. Six terms in the right eye were significantly different from zero, those being $j = 10$ ($t=4.28$, $P<0.0001$), 11 ($t=3.10$, $P=0.003$), 12 ($t=9.83$, $P<0.0001$), 14 ($t=6.61$, $P<0.0001$), 15 ($t=4.05$, $p=0.0001$) and 20 ($t=4.20$, $P<0.0001$), but the mean amplitude of four of them ($j=10$, 11, 15 and 20) was around 0.01 μm . In the left eye, five terms were found to be significantly different from zero: $j=6$ ($t=3.10$, $P=0.003$), 8 ($t=3.70$, $P=0.0004$), 12 ($t=9.74$, $P<0.0001$), 14 ($t=6.92$, $P<0.0001$), and 20 ($t=3.69$, $P=0.0004$). Only $j=20$ had a mean amplitude of around 0.01 μm , the rests were much higher in amplitude (>0.035 μm). The terms showing significantly different values between the two eyes were $j=8$ ($t=4.31$, $P<0.0001$) and 10 ($t=4.65$, $P<0.0001$).

Mean Higher Order Zernike Aberrations for Myopes

Mean higher order aberrations in the anterior cornea and the whole eye for 196 myopes were calculated by averaging the aberrations across the right and left eyes. Instead of 3 terms, as shown for the emmetropes in *table 2*, 8 corneal Zernike modes were found to be significantly different from zero for the myopes, and those were $j = 6, 7, 11, 12, 14, 16, 17$, and 20. For the whole eye, 5 terms ($j = 10, 12, 14, 15$, and 16) were significantly different from zero. Three non-zero aberration terms, $j = 12, 14$ and 16, in both the anterior cornea and the whole eye were observed. As in the emmetropic group, mean spherical aberration in the myopic group was positive both for the anterior cornea and for the whole eye, but with greater amplitude in the cornea than in the whole eye. Unlike the emmetropic group, the mean aberration of $j = 6$ in the whole eye for the myopic group was not significantly different from zero. All the non-zero aberrations in the 5th order were very small in amplitude ($<=0.01\mu\text{m}$).

Table 4 shows the mean Zernike aberrations for the myopes, but where the signs corresponding to the left eye have been flipped. Once the signs were flipped, only three ($j=9, 13$ and 15) out of the 15 terms in the cornea and four ($j=6, 7, 13$ and 17) out of the 15 terms in the whole eye were not significantly different from zero.

Mean RMS value for all 392 myopic eyes was 0.389 μm in the anterior cornea and 0.291 μm in the whole eye. With spherical aberration excluded, the mean RMS values decreased to 0.326 μm and 0.258 μm in the anterior cornea and in whole eye, respectively. Without flipping the signs, the RMS value associated to the mean higher-order Zernike aberrations was 0.199 μm (in the cornea) and 0.084 μm (in the whole eye) when spherical aberration was included, and 0.061 μm (in the cornea) and 0.028 μm (in the whole eye) when spherical aberration was excluded. Once the signs were flipped, the RMS value associated to the mean higher-order Zernike aberrations went up to 0.254 μm (in the cornea) and 0.101 μm (in the whole eye) with spherical aberration included, and 0.169 μm (in the cornea) and 0.062 μm (in the whole eye) with spherical aberration excluded.

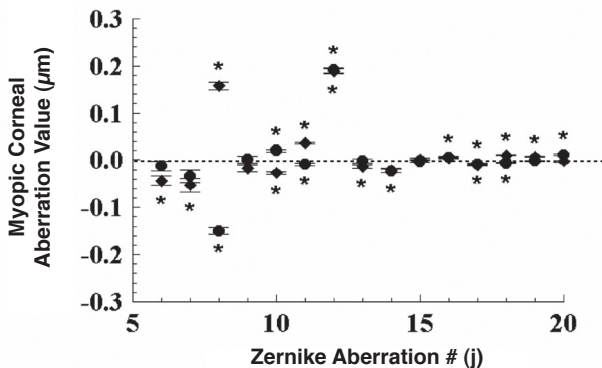
Figure 3 shows the mean higher-order Zernike aberration terms in the anterior cornea for the right (solid circles) and

TABLE 4

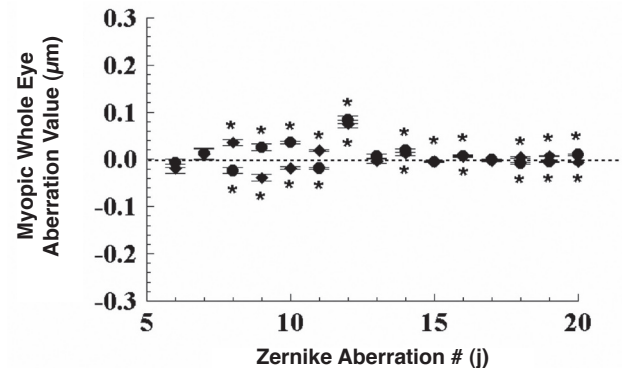
Mean higher-order Zernike aberrations of the anterior cornea and of the whole eye over a 6 mm pupil area for 196 young myopes, with signed coefficients averaged for both the right and left eyes but the signs flipped for the y-axis asymmetrical Zernike coefficients in the left eye

	Anterior Cornea			Whole Eye		
	Mean \pm SD (μm)	95% CI (μm)	<i>P</i>	Mean \pm SD (μm)	95% CI (μm)	<i>P</i>
j=6 (Z_3^{-3})	-0.028 \pm 0.138	(-0.042, -0.015)	<0.0001***	-0.014 \pm 0.136	(-0.027, -0.000)	0.048
j=7 (Z_3^{-1})	-0.043 \pm 0.196	(-0.062, 0.024)	<0.0001***	0.012 \pm 0.161	(-0.004, 0.028)	0.149
j=8 (Z_3^1)	-0.154 \pm 0.110	(-0.165, -0.143)	<0.0001***	-0.030 \pm 0.089	(-0.039, -0.021)	<0.0001***
j=9 (Z_3^3)	0.008 \pm 0.104	(-0.001, 0.019)	0.085	0.032 \pm 0.100	(0.022, 0.042)	<0.0001***
j=10 (Z_4^{-4})	0.023 \pm 0.037	(0.020, 0.027)	<0.0001***	0.027 \pm 0.036	(0.024, 0.031)	<0.0001***
j=11 (Z_4^{-2})	-0.023 \pm 0.033	(-0.026, -0.020)	<0.0001***	-0.019 \pm 0.032	(-0.022, -0.016)	<0.0001***
j=12 (Z_4^0)	0.190 \pm 0.076	(0.182, 0.197)	<0.0001***	0.079 \pm 0.111	(0.068, 0.090)	<0.0001***
j=13 (Z_4^2)	-0.008 \pm 0.058	(-0.014, -0.002)	0.005	0.001 \pm 0.056	(-0.004, 0.007)	0.612
j=14 (Z_4^4)	-0.023 \pm 0.052	(-0.028, -0.017)	<0.0001***	0.016 \pm 0.047	(0.011, 0.020)	<0.0001***
j=15 (Z_5^{-5})	-0.000 \pm 0.029	(-0.003, 0.003)	0.856	-0.005 \pm 0.025	(-0.008, -0.003)	<0.0001***
j=16 (Z_5^{-3})	0.005 \pm 0.025	(0.002, 0.0076)	0.0001**	0.007 \pm 0.026	(0.004, 0.009)	<0.0001***
j=17 (Z_5^{-1})	-0.010 \pm 0.027	(-0.012, -0.007)	<0.0001***	-0.002 \pm 0.030	(-0.005, 0.001)	0.189
j=18 (Z_5^1)	-0.008 \pm 0.014	(-0.010, -0.007)	<0.0001***	-0.006 \pm 0.018	(-0.008, -0.005)	<0.0001***
j=19 (Z_5^3)	-0.005 \pm 0.018	(-0.007, -0.003)	<0.0001***	-0.006 \pm 0.018	(-0.008, -0.005)	<0.0001***
j=20 (Z_5^5)	0.007 \pm 0.027	(0.004, 0.009)	<0.0001***	0.008 \pm 0.024	(0.005, 0.010)	<0.0001***

Significance was corrected for multi-comparison with * standing for $P < 0.05$ (0.0033), ** for $P < 0.01$ (0.00067), and *** for $P < 0.001$ (0.000067) level respectively.

**FIGURE 3**

Mean higher-order Zernike aberrations of the anterior cornea over a 6.0 mm pupil area for the right (solid circles) and left eyes (solid diamonds) of 196 myopes.

**FIGURE 4**

Mean higher-order Zernike aberrations of the whole eye over a 6.0 mm pupil area for the right (solid circles) and left eyes (solid diamonds) of 196 myopes.

left eyes (solid diamonds) of the 196 myopic subjects. Nine out of the 15 Zernike aberration terms corresponding to the right eye were significantly deviated from zero, among them eight ($j = 8, 10, 11, 12, 14, 17, 18,$ and 20) had a t -test value greater than 4.15 ($P < 0.0001$). Another one $j = 16$ had a t value equal to 3.23 ($P = 0.0015$). As for the left eye, eleven Zernike terms ($j = 6, 7, 8, 10, 11, 12, 13, 14, 17, 18,$ and 19) were significantly different from zero, and most of them had a t value greater than 4.30 ($P < 0.0001$) except for $j = 7$ and 13 , which had a t value between 3.5 and 3.8 ($P < 0.001$). Meanwhile, six terms ($j = 8, 10, 11, 18, 19,$ and 20) were significantly different when comparing left and right eyes, with t value being greater than 5.0 ($P < 0.0001$).

Figure 4 shows the mean higher-order Zernike aberration terms corresponding to the whole eye in both the right and left eyes for the 196 young myopes. Eleven out of the fifteen Zernike aberrations were different from zero in the right eye, and seven of them ($j = 10, 11, 12, 14, 16, 18,$ and 20) had t values greater than 4.07 ($P < 0.0001$). The other 4 terms ($j = 8, 9, 15,$ and 19) had t values that ranged from 3.55 to 3.82 ($P < 0.001$). Ten Zernike aberrations in the left eye were significantly different from zero, and six of them ($j = 8, 9, 10, 11, 12,$ and 19) had t values greater than 5.48 ($P < 0.0001$). The other 4 terms ($j = 14, 16, 18,$ and 20) had t values between 3.13 and 3.65 ($P < 0.003$). For seven higher-order aberration terms the values for the right and left eyes differed signifi-

cantly: $j = 8, 9, 10, 11, 18, 19,$ and 20 ($t > 6.3, P < 0.0001$ for all of them).

DISCUSSION

We have found that five out of the fifteen higher-order Zernike aberrations (3rd to 5th orders) in the whole eye of 75 young emmetropes, in addition to the spherical aberration, had mean levels significantly different from zero when signed Zernike aberrations were averaged across the right and left eyes of the same individual (Table 2). Three more terms become statistically different from zero as the signs of y-axis asymmetrical Zernike aberrations in the left eye were flipped (Table 3). The results indicate that, on average, the emmetropic population is not free from higher-order Zernike aberrations. This is consistent with the study on emmetropes by Plainis and Pallikris¹⁶ (with three statically non-zero terms including spherical aberration), although in this study more higher-order terms (six terms) were found to be statistically non-zero. Regarding the mean RMS associated to higher-order aberrations for all emmetropes (0.336 μm with spherical aberration and 0.284 μm without spherical aberration), the RMS of the mean Zernike higher-order aberrations of the emmetropic group was about 46% (0.155/0.336 with spherical aberration) and 25% (0.07/0.284 without spherical aberration) in amount respectively when sign was not flipped, and 47% (0.159/0.336 with spherical aberration) and 28% (0.080/0.284 without spherical aberration) respectively when sign was flipped. The results suggests that the mean higher-order Zernike aberrations in a young emmetropic population are not small and, thus, should not be overlooked. Therefore, the human eye, even in the best case of emmetropia, has not reached yet the condition of being free of higher-order aberrations.

Regarding to the whole eye aberrations for the myopic group, five higher-order Zernike terms, including spherical aberration, were statistically non-zero when signs were not flipped, increasing to eleven terms that were statistically non-zero when the signs were flipped (Table 4). The number of statistically non-zero Zernike aberrations for the myopic group was, in this study, very close to the value obtained for the emmetropic group. The subjects in Wang and Koch's⁹ study were basically myopes and also from an older age, as compared to the subjects in this study. They found that 2/3 of the higher-order Zernike terms were statistically non-zero when the signs were not flipped, which is more than what was observed in this study (5 terms). This might be due to an age difference. But, Carkeet and colleagues⁸ also found 2/3 statistically non-zero higher-order terms in their subjects, who were of a younger age. Apparently, further study is needed in order to clarify this point.

In the three aforementioned early studies they used laboratory-constructed wavefront sensors,^{4,6} refraction of their subjects was a bit biased towards myopia, with refractive errors compatible both with that of the myopes in the current study and also those in the other two later studies.^{9,15} However, only spherical aberration was found to be significantly differing from zero. The reasons behind this inconsistency are not clear to us. But, as for Thibos et al's study,⁴ a possible factor might be that their subject's pupil was dilated

while we tested the natural pupil. After dilation, the pupil center could be shifted³¹⁻³⁵ and become closer to the line of sight. This shift of the pupil center toward the line of sight could make the structure of higher-order aberrations more symmetrical with respect to the line of sight, thus systematically reducing the values associated to the asymmetric higher-order aberrations of the population under study.

Sign flipping of y-axis asymmetric Zernike aberrations in the left eye resulted in more Zernike terms being statistically different from zero in both the emmetropic and the myopic groups (Tables 3 and 4). Analysis of the mean Zernike aberrations taking the two eyes of each individual separately also showed more Zernike terms being significantly different from zero (Figures 1-4) as compared to the results when both left and right eyes were analyzed together. The results indicate that more systematical higher-order aberrations are revealed when the right and the left eyes are considered separately. Because the increase in non-zero Zernike terms with the sign flipping or with eye separation is related to the bilateral symmetry occurring between the two eyes, the systematical higher-order aberrations in a given population must be partially determined by factors which also control this bilateral symmetry of the wavefront aberrations between the two eyes. Obviously this is an interesting issue for further study.

Several statistically non-zero higher-order Zernike aberrations in the anterior cornea were observed in either the emmetropic or the myopic group no matter the signs were flipped or not (Tables 2-4). A similar result, without sign flipping, was also reported by Wang et al.³⁶ In our study, some of the non-zero terms were simultaneously observed in both the anterior cornea and the whole eye, such as $j=6, 12$ and 13 for emmetropes, even without sign flipping (Table 2). The results suggest that the anterior cornea plays an important role in determining the systematical aberrations in the whole eye. Meanwhile, internal optics, including the posterior cornea and the lens, also contribute to the systematical whole-eye aberrations because some of the statistically non-zero Zernike aberration terms were observed in the whole eye but not in the anterior cornea, e.g. $j=14, 15$ and 17 (Table 2). Wavefront aberrations in the anterior cornea were partially compensated by interior optics.^{18,20-23} This is true for this study since the amplitude of the Zernike aberration terms for the whole eye was for most terms smaller than that obtained for the anterior cornea alone, especially for the relatively lower-order Zernike terms (3rd to 4th). The RMS values in the whole eye were also reduced. However, the basic distribution of systematical higher-order aberrations in the whole eye did not change much relative to that obtained for the anterior cornea.

A commercial aberrometer was used to measured whole-eye aberrations in this study. It might be concerned that the systematical higher-order aberrations observed in both the emmetropic and the myopic groups were due to instrumental error because the commercial model was as accurate as the laboratory-constructed systems.^{4,6} This is a problem for all aberrometers available in the market, since so far we have no standard to test the accuracy of the aberrometers against, when it comes to measuring higher-order aberrations. However, in this study, we found that many of the higher-

order aberrations were not significantly different from zero in both the anterior cornea and the whole eye simultaneously. Bearing in mind that the corneal aberration pattern was obtained using a different instrument, the coincidence of getting a similar pattern of wavefront aberrations from two different instruments largely suggests that the hypothesis of an instrumental error is quite unlikely.

This study indicates that the population is not free of higher-order aberrations. This means that the human eye has not reached yet the perfect optical condition during the process of evolution. An interesting question, therefore, is whether or not this systematical higher-order aberrations are of some biological significance for the visual performance of the human eye. While visual acuity was found to be improved as the higher-order aberrations were completely corrected in several recent studies with adaptive optics,³⁷⁻⁴³ aberration as a cue for accommodation was also demonstrated in some subjects.⁴⁴ Clearly, further studies on this issue are expected. In clinical practices, it might be needed to think more about what the goal should be: to correct wavefront aberrations completely or not, before a fully understanding of the significance of higher-order aberrations in the eye was established.

REFERENCES

- Applegate RA. Glenn Fry Award Lecture 2002: Wavefront sensing, ideal corrections, and visual performance. *Optom Vis Sci* 2004;81:167-177.
- Thibos LN. The optics of wavefront sensing. *Ophthalmol Clin North Am*. 2004;17:111-117.
- Charman WN. The Charles F. Prentice Award Lecture 2005: Optics of the human eye: progress and problems. *Optom Vis Sci*. 2006;83:335-345.
- Thibos LN, Hong X, Bradley A, Cheng X. Statistical variation of aberration structure and image quality in a normal population of healthy eyes. *J Opt Soc Am A*. 2002;19:2329-2348.
- Porter J, Guirao A, Cox IG, Williams DR. Monochromatic aberrations of the human eye in a large population. *J Opt Soc Am A*. 2001;18:1793-1803.
- He, JC, Sun P, Held R, Thorn F, Sun X, Gwiazda J. Wavefront aberrations in eyes of emmetropic and moderately myopic school children and young adults. *Vision Res*. 2002;42:1063-1070.
- Castejón-Mochón JF, López-Gil N, Benito A, Artal P. Ocular wavefront aberration statistics in a normal young population. *Vision Res*. 2002;42:1611-1617.
- Carkeet A, Luo HD, Tong L, Saw SM, Tan DTH. Refractive error and monochromatic aberrations in Singaporean children. *Vision Res*. 2002;42:1809-1824.
- Wang L, Koch DD. Ocular high-order aberrations in individuals screened for refractive surgery. *J Cataract Refract Surg*. 2003;29:1896-1903.
- Brunette I, Bueno JM, Parent M, Hamam H, Simonet P. Monochromatic aberrations as a function of age, from childhood to advanced age. *Invest Ophthalmol Vis Sci*. 2003;44:5438-5446.
- Amano S, Amano Y, Yamagami S, et al. Age-related changes in corneal and ocular higher-order wavefront aberrations. *Am J Ophthalmol*. 2004;137:988-992.
- Cheng H, Barnett JK, Vilupuru AS, et al. A population study on changes in wave aberrations with accommodation. *J Vis*. 2004; 4: 272-280. <http://journalofvision.org/4/4/3/>
- Netto MV, Ambrosio Jr R, Shen TT, Wilson SE. Wavefront analysis on normal refractive surgery candidates. *J Cataract Refract Surg*. 2005;21:332-338.
- Zadok D, Levy Y, Segal O, Barkana Y, Morad Y, Avni I. Ocular higher-order aberrations in myopia and skiascopic wavefront repeatability. *J Cataract Refract Surg*. 2005;31:1128-1132.
- Wei RH, Lim L, Chan WK, Tan DTH. Higher order ocular aberrations in eyes with myopia in a Chinese population. *J Refract Surg*. 2006;22:695-702.
- Plainis S, Pallikaris IG. Ocular monochromatic aberration statistics in a large emmetropic population. *J Mod Opt*. 2008;55:759-772.
- Salmon TO, Van de Pol C. Evaluation of a clinical aberrometer for lower-order accuracy and repeatability, higher-order repeatability, and instrument myopia. *Optometry*. 2005;76:461-472.
- He JC, Gwiazda J, Thorn F, Held R. Wave-front aberrations in the anterior corneal surface and the whole eye. *J Opt Soc Am A*. 2003;20:1155-1163.
- Qu J, Lu F, Wu J, et al. Wavefront aberration and its association with intraocular pressure and central corneal thickness in myopic eyes. *J Cataract Refract Surg*. 2007;33:1447-1454.
- Artal P, Guirao A. Contributions of the cornea and the lens to the aberrations of the human eye. *Opt Letters*. 1998; 23:1713-1715.
- Artal P, Guirao A, Berrio E, Williams DR. Compensation of corneal aberrations by internal optics in the human eye. *J Vis*. 2001;1:1-8. <http://journalofvision.org/1/1/1/>
- Artal P, Berrio E, Guirao A, Piers P. Contribution of the cornea and internal surfaces to the change of ocular aberrations with age. *J Opt Soc Am A*. 2002;19:137-143.
- Kelly JE, Mihashi T, Howland HC. Compensation of corneal horizontal/vertical astigmatism, lateral coma, and spherical aberration by internal optic of the eye. *J Vis*. 2004;4:262-271. <http://journalofvision.org/4/4/2/>.
- Thibos LN, Applegate RA, Schwiegerling JT, Webb R, VSIA Standards Taskforce Members. Standards for reporting the optical aberrations of eye. *Trends in Optics and Photonics, Vision Science and Its Applications*. 2000;35:232-244.
- Liang J, Williams DR. Aberrations and retinal image quality of the normal human eye. *J Opt Soc Am A*. 1997;14:2873-2883.
- Smolek MK, Klyce SD, Sarver EJ. Inattention to nonsuperimposable midline symmetry causes wavefront analysis error. *Arch Ophthalmol*. 2002;120:439-447.
- Thibos LN, Bradley A, Hong X. A statistical model of the aberration structure of normal, well-corrected eyes. *Ophthalmic Physiol Opt*. 2002;22:427-433.
- Wang L, Dai E, Koch DD, Nathoo A. Optical aberrations of the human anterior cornea. *J Cataract Refract Surg*. 2003;29:1514-1521.
- Wang L, Santaella RM, Booth M, Koch DD. Higher-order aberrations from the internal optics of the eye. *J Cataract Refract Surg*. 2005;31:1512-1519.
- Lu F, Wu JX, Qu J, et al. Association between offset of the pupil center from the corneal vertex and wavefront aberration. *J Optom*. 2008;1:8-13. <http://dx.doi.org/10.3921/joptom.2008.8>
- Walsh G. The effect of mydriasis on papillary centration of the human eye. *Ophthalmic Physiol Opt*. 1988;8:178-182.
- Wilson MA, Campbell MCW, Simonet P. Change of pupil centration with change in illumination and pupil size; The Julius F. Neumuller Award in Optics, 1989. *Optom Vis Sci*. 1992;69:129-136.
- Wyatt HJ. The form of the human pupil. *Vision Res*. 1995;35:2021-2036.
- Yang Y, Thompson K, Burns BA. Pupil location under mesopic, photopic, and pharmacologically dilated conditions. *Invest Ophthalmol Vis Sci*. 2002;43:2508-2512.
- Porter J, Yoon G, Lozano D, et al. Aberrations induced in wavefront-guided laser refractive surgery due to shifts between natural and dilated pupil center locations. *J Cataract Refract Surg*. 2006;32:21-32.
- Wang L, Dai E, Hoch DD, Nathoo A. Optical aberrations of the human anterior cornea. *J Cataract Refract Surg*. 2003;29:1514-1521.
- Yoon G, Jeong TM, Cox IG, Williams DR. Vision improvement by correcting higher-order aberrations with phase plates in normal eyes. *J Refract Surg*. 2004;20:S523-S527.
- Williams D, Yoon GY, Porter J, Guirao A, Hofer H, Cox I. Visual benefit of correcting higher order aberrations of the eye. *J Refract Surg*. 2000;16:S554-S559.
- Yoon GY, Williams DR. Visual performance after correcting the monochromatic and chromatic aberrations of the eye. *J Opt Soc Am A Opt Image Sci Vis*. 2002;19:266-275.
- Rocha KM, Vabre L, Harms F, Chateau N, Krueger RR. Effects of Zernike wavefront aberrations on visual acuity measured using electromagnetic adaptive optics technology. *J Refract Surg*. 2007;23:953-959.
- Piers PA MS, Prieto PM, Gorceix N, Artal P. Use of adaptive optics to determine the optimal ocular spherical aberration. *J Cataract Refract Surg*. 2007;33:1721-1726.
- Rossi EA, Weiser P, Tarrant J, Roorda A. Visual performance in emmetropia and low myopia after correction of high-order aberrations. *J Vis*. 2007;7:1-14. <http://journalofvision.org/7/8/14/>
- Legras R, Rouger H. Calculations and measurements of the visual benefit of correcting the higher-order aberrations using adaptive optics technology. *J Optom*. 2008;1:22-29.
- Chen L, Kruger PB, Hofer H, Singer B, Williams D. Accommodative with higher-order monochromatic aberrations corrected with adaptive optics. *J Opt Soc Am A*. 2006;23:1-8.